

Cite this: *Chem. Commun.*, 2012, **48**, 8694–8696

www.rsc.org/chemcomm

COMMUNICATION

Mapping protein-specific micro-environments in live cells by fluorescence lifetime imaging of a hybrid genetic-chemical molecular rotor tag†

Evangelos Gatzogiannis,‡§ Zhixing Chen,§ Lu Wei, Richard Wombacher,¶ Ya-Ting Kao, Grygorii Yefremov, Virginia W. Cornish|| and Wei Min*

Received 1st May 2012, Accepted 6th July 2012

DOI: 10.1039/c2cc33133k

The micro-viscosity and molecular crowding experienced by specific proteins can regulate their dynamics and function within live cells. Taking advantage of the emerging TMP-tag technology, we present the design, synthesis and application of a hybrid genetic-chemical molecular rotor probe whose fluorescence lifetime can report protein-specific micro-environments in live cells.

The micro-mechanical environment of proteins inside live cells and its effect on key biochemical processes are important yet unresolved issues in cell biology.¹ Intracellular viscosity plays an important role in biochemical processes such as signal transduction, nuclear envelope function, chromatin localization, ribonucleoprotein assembly and diffusion of reactive oxygen species.^{2–4} Changes in viscosity at a sub-cellular level have been related to a number of diseases and pathologies.⁵ The determination of local viscosities and other micro-environmental parameters within the nucleus and other critical cellular organelles in live cells is of great interest.^{2–13}

Experimentally, intracellular viscosity has been measured by tracking fluorophore diffusion, fluorescence correlation spectroscopy, and fluorescence recovery after photobleaching.^{6–9} These methods, however, suffer from long acquisition times (~100 s) and cannot report the spatial variation of micro-viscosities in a rapid imaging mode compatible with live cell imaging. Recently, fluorescent molecular rotors have emerged as novel, environmentally-sensitive probes capable of generating high-resolution images of the spatial distribution of micro-viscosities in a biological sample.^{10–13} However, the current molecular rotor approach has low organelle specificity and does not allow for protein-specific micro-environment measurements.^{10–13} This missing protein-specific information, if obtainable, would enhance our understanding of the dynamics and function of

proteins inside cells. The fluorescence properties (intensity, lifetime and quantum yield) of genetically-encoded fluorescent proteins (such as GFP) are, unfortunately, insensitive to the medium viscosity because of shielding and isolation of the chromophore from the surroundings by the protein β -barrels.¹⁴ In addition, fluorescence anisotropy cannot report the viscosity experienced by stationary proteins (*e.g.*, H2B) inside cells. In the present study, we explored the emerging chemical tagging technology and developed a hybrid genetic-chemical eDHFR–TMP–Cy3 rotor tag to report protein-specific micro-viscosity by fluorescence lifetime imaging microscopy (FLIM).

The emerging chemical tagging technology has offered a route to selectively label a protein of interest *in vivo* with an organic fluorescent dye in a genetically encoded manner.¹⁵ The TMP-tag takes advantage of a strong non-covalent interaction between *E. coli* dihydrofolate reductase (eDHFR) and trimethoprim (TMP) which displays a nano-molar affinity, in addition to a recently developed covalent version.¹⁶ It stands out as one of the few tags that work inside living cells with a high labeling specificity and efficiency.¹⁶ The DNA sequence that encodes the small (18 kDa) and monomeric eDHFR is genetically fused to a protein of interest, and then a highly cell-permeable TMP–dye conjugate is introduced. The TMP–dye conjugate diffuses into the cell and recognizes the eDHFR fusion protein. By incorporating bright organic fluorophores such as Atto dyes, the TMP-tag has demonstrated its utility in super-resolution microscopy and single molecule biophysics.^{17,18}

We selected Cy3 as the conjugation probe because of its environment-sensitive fluorescence lifetime. The photophysical properties of Cy3 have been well studied.^{19–22} As shown in Fig. 1a, after excitation, in addition to the radiative decay pathway generating fluorescence, Cy3 can also isomerize from the *trans*- to the *cis*-configuration through a torsional motion, bringing Cy3 back to its ground state without photon emission. As a result, the measurable fluorescence lifetime, τ ,

$$\tau(\eta) = \frac{1}{k_{sp} + k_{nr}(\eta) + k_{i.c.}}$$

is the inverse sum of the radiative decay rate constant of spontaneous emission k_{sp} , the non-radiative decay rate, k_{nr} , which is sensitive to the medium viscosity, η , and direct

Department of Chemistry, Columbia University, 3000 Broadway and 119th Street, New York, NY, USA. E-mail: wm2256@columbia.edu

† Electronic supplementary information (ESI) available: Synthesis of TMP–Cy3, additional spectroscopic tests, FLIM and microscopy instrumentation. See DOI: 10.1039/c2cc33133k

‡ Current address: National Institute of Standards and Technology, Gaithersburg, MD 20899, USA.

§ These authors contributed equally to the work.

¶ Current address: Institute of Pharmacy and Molecular Biotechnology, Heidelberg University, Heidelberg, Germany.

|| V. W. C. holds patents on the TMP-tag technology, and the technology is licensed and commercialized by Active Motif.

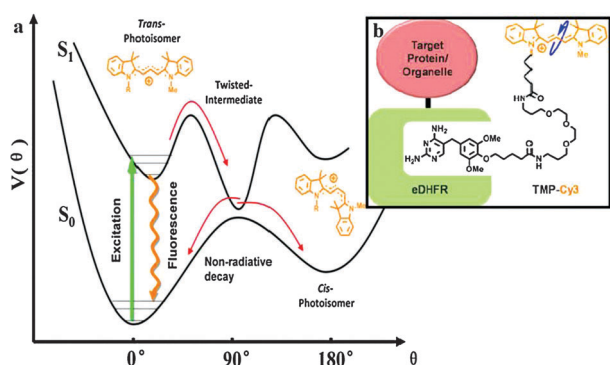


Fig. 1 (a) Cy3 photophysics and (b) design of the eDHFR–TMP–Cy3 probe.

internal conversion from the excited state, $k_{i.c.}$ ²³ In a low-viscosity environment such as in water, the non-radiative photo-isomerization pathway of Cy3 is dominant and the fluorescence lifetime is short (<0.2 ns). A viscous medium will hinder the rate of torsional motion on the potential surface of the excited state and prolong the fluorescence lifetime, as explained by the Kramers theory on barrier crossing.²⁴ Although cyanine derivatives have been widely used in applications from *in vitro* protein labeling to *in vivo* animal diagnostic imaging,²⁵ the environmentally-sensitive photo-physical properties of cyanine derivatives have not been explored until recently. Notably, in two recent *in vitro* single-molecule studies, Cy3 was exploited as a novel local reporter to probe real-time protein binding onto DNA.^{26,27} These emerging results encourage us to harness the environmental sensitivity of Cy3 in live cells for imaging.

We developed a TMP–Cy3 probe for live cell imaging (Fig. 1b). A cell-permeable TMP–Cy3 conjugate was synthesized by modularized conjugation of TMP–NH₂ with a sulfonate-free version of Cy3 (Scheme S1, Fig. S1, ESI†). A flexible polyethylene glycol (PEG) spacer was introduced between TMP and Cy3 to minimize the potential influence of the eDHFR protein on the nearby Cy3 probe.

TMP–Cy3 was tested as an environment sensor *in vitro* before its use in cellular experiments (Fig. 2). Fluorescence intensity and lifetime measurements on TMP–Cy3 were carried out in glycerol–water solutions with different viscosities. All measurements were made on a home-built frequency-domain FLIM microscope (ESI†). The fluorescence lifetime of TMP–Cy3

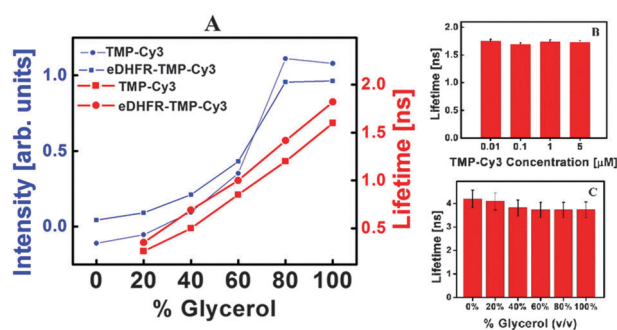


Fig. 2 Fluorescence intensity and lifetime of TMP–Cy3 and eDHFR–TMP–Cy3 (A). Concentration independence of TMP–Cy3 (B), rhodamine insensitivity to viscosity (C).

increases from 0.2 ± 0.1 ns to 1.6 ± 0.2 ns with increasing glycerol volume fraction from 20% to 100%, consistent with a restriction of torsional motion and a hindered non-radiative decay. The fluorescence of TMP–Cy3 and eDHFR–TMP–Cy3 was compared in order to examine the potential perturbation effect of the protein on the nearby fluorophore. As shown in Fig. 2A, a minimal effect of the eDHFR binding on the lifetime and brightness of TMP–Cy3 was observed, most likely attributed to the long PEG spacer designed between TMP and Cy3.

For use as a specific micro-environment sensor inside cells, TMP–Cy3 should have negligible interactions with DNA, proteins and ions. Indeed, this is the case, as confirmed by *in vitro* spectroscopy experiments of TMP–Cy3 in solutions of varying DNA, bovine serum albumin (BSA) and NaCl concentrations (ESI†). TMP–Cy3, however, does weakly interact with micelles formed by SDS (Sodium Dodecyl Sulfate). The fluorescence lifetime of TMP–Cy3 is independent of the fluorophore concentration (Fig. 2B), which is an advantage in quantitative FLIM studies as the concentration of the fluorophore within live cells is not well controlled. At concentrations from 10 nM to 5 μ M, the fluorescence lifetime of TMP–Cy3 is constant (Fig. 2B). Rhodamine 6G, a common non-rotor dye, has a constant fluorescence lifetime with varying glycerol concentrations (Fig. 2C), underscoring the necessity of flexible rotor tags for viscosity imaging.

Encouraged by the *in vitro* experiments, we moved on to cellular experiments to evaluate the ability of TMP–Cy3 to map local micro-environments. To target the molecular rotor to the cell nucleus, eDHFR was fused to histone H2B protein. We also studied the cytosol environment in the vicinity of the cell membrane by anchoring eDHFR with a plasma membrane localization signal (PMLS). We transiently transfected HEK 293T cells with plasmids encoding H2B–eDHFR or PMLS–eDHFR fusion protein, then incubated the cells with our synthesized, cell-permeable TMP–Cy3 for 10 min, and imaged them. The H2B–eDHFR images show minor degrees of non-specific granular-shaped binding of TMP–Cy3 to lipid-rich organelles.²⁸ Nevertheless, oval-shaped nuclei with distinct

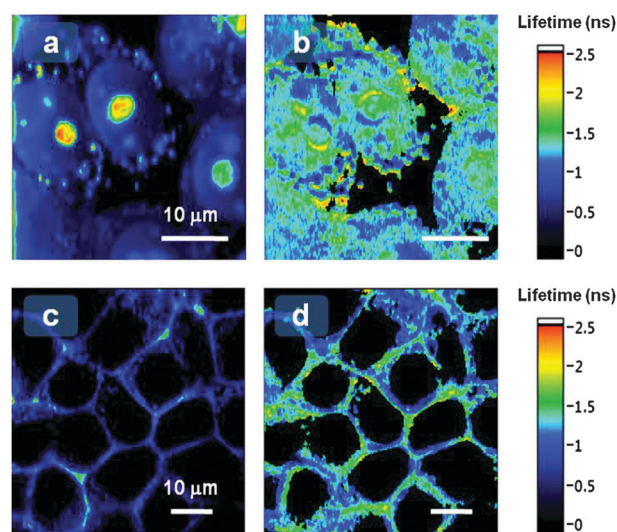


Fig. 3 Fluorescence intensity (a, c) and fluorescence lifetime (b, d) images of H2B–eDHFR–TMP–Cy3 (a and b) and PMLS–eDHFR–TMP–Cy3 (c and d) in live cells.

nucleoli were clearly observed (Fig. 3a and b). Characteristic plasma membrane patterns were observed in cells expressing PMLS-eDHFR (Fig. 3c). Therefore, this approach would be suitable for monitoring the nuclear and plasma membrane environment as non-specific staining was minor inside the nucleus and near the plasma membrane.

FLIM microscopy was used to image the distributions of local environments experienced by H2B within the cell nuclei and cytosol viscosities near the cell membrane. FLIM imaging (Fig. 3a) revealed that the nuclear viscosity is high, comparable to glycerol solutions from 50% volume fraction (~ 1 ns) up to considerably higher values in certain regions (> 2.0 ns). The average lifetime over the two brightest nuclei with clearly visible nucleoli to the left-of-center in Fig. 3a is 1.4 ± 0.3 ns, indicative of a viscous and crowded environment. Our lifetime measurements correspond to average viscosities of around 60–70 cP within the nucleus, comparable to other reports.¹³ There is also remarkable heterogeneity in the distributions of the measured micro-environment, offering information not available from the confocal fluorescence intensity image. This heterogeneity may be related to the recently reported heterogeneous level of chromatin compaction detected by fluorescence anisotropy imaging of H2B-EGFP.²⁹ FLIM images were also captured for TMP-Cy3 labeled PMLS-eDHFR in the vicinity of cell membranes (Fig. 3d). In this scenario, the average lifetime is typically 0.9 ± 0.2 ns, indicating a relatively less viscous and crowded area of the cell cytoplasm compared to the nucleus experienced by H2B.

In conclusion, we developed a hybrid genetic-chemical molecular rotor tag (eDHFR-TMP-Cy3) to measure protein-specific local environments in live cells using FLIM. Although we only used the TMP-tag, the same Cy3 rotor moiety can be readily applied to other chemical tagging techniques such as the SNAP, CLIP, and HaloTag.^{15,30} This methodology, with its good genetically-encoded specificity, high spatial-temporal resolution and simple interpretation, could provide valuable mechanistic information about protein function in the complex and constantly changing cellular environment. For example, the observed heterogeneous micro-environment could have broader implications in understanding chromatin condensation and transcription control within live cells.³¹ Chemical tags can be engineered with arbitrary open-structure biophysical probes that are exposed to their surroundings and can sense the local environment more sensitively than regular fluorescent proteins. To our knowledge, this advantageous aspect of chemical tags has been largely unexplored. This protein/organelle specific FLIM technique should be useful for evaluating a wider variety of protein or organelle-specific cellular micro-environments.

This work was supported by the National Institutes of Health (U54 GM087519 and RC1GM091804 to V. W. C.) and by the start up funds from Columbia University (to W. M.). We thank Dr Steffen Jockusch for experimental assistance.

Notes and references

- 1 K. E. Handwerger and J. G. Gall, *Trends Cell Biol.*, 2006, **16**, 19–26.
- 2 I. Lang, M. Scholz and R. Peters, *J. Cell Biol.*, 1986, **102**, 1183–1190.
- 3 W. F. Marshall, A. Straight, J. F. Marko, J. Swedlow, A. Dernburg, A. Belmont, A. W. Murray, D. A. Agard and J. W. Sedat, *Curr. Biol.*, 1997, **7**, 930–939.
- 4 T. Kues, A. Dickmanns, R. Lührmann, R. Peters and U. Kubitscheck, *Proc. Natl. Acad. Sci. U. S. A.*, 2001, **98**, 12021–12026.
- 5 K. Luby-Phelps, *Int. Rev. Cytol.*, 2000, **192**, 189–221.
- 6 J. W. Wojcieszyn, R. A. Schlegel, E. S. Wu and K. A. Jacobson, *Proc. Natl. Acad. Sci. U. S. A.*, 1981, **78**, 4407–4410.
- 7 L. Liang, X. Wang, D. Xing, T. Chen and W. R. Chen, *J. Biomed. Opt.*, 2009, **14**, 0240131.
- 8 O. Seksek, J. Biwersi and A. S. Verkman, *J. Cell Biol.*, 1997, **138**, 131–142.
- 9 D. Grünwald, R. M. Martin, V. Buschmann, D. P. Bazett-Jones, H. Leonhardt, U. Kubitscheck and M. C. Cardoso, *Biophys. J.*, 2008, **94**, 2847–2858.
- 10 M. A. Haidekker, T. P. Brady, D. Lichlyter and E. A. Theodorakis, *J. Am. Chem. Soc.*, 2006, **128**, 398–399.
- 11 M. K. Kuimova, S. W. Botchway, A. W. Parker, M. Balaz, H. A. Collins, H. L. Anderson, K. Suhling and P. R. Ogilby, *Nat. Chem.*, 2009, **1**, 69–73.
- 12 X. Peng, Z. Yang, J. Wang, J. Fan, Y. He, F. Song, B. Wang, S. Sun, J. Qu, J. Qi and M. Yan, *J. Am. Chem. Soc.*, 2011, **133**, 6626–6635.
- 13 M. K. Kuimova, G. Yahioglu, J. A. Levitt and K. Suhling, *J. Am. Chem. Soc.*, 2008, **130**, 6672–6673.
- 14 K. Suhling, J. Siegel, D. Phillips, P. M. French, S. Lévêque-Fort, S. E. Webb and D. M. Davis, *Biophys. J.*, 2002, **83**, 3589–3595.
- 15 C. Jing and V. W. Cornish, *Acc. Chem. Res.*, 2011, **44**, 784–792.
- 16 L. W. Miller, Y. Cai, M. P. Sheetz and V. W. Cornish, *Nat. Methods*, 2005, **2**, 255–257.
- 17 R. Wombacher, M. Heidebreder, S. van de Linde, M. P. Sheetz, M. Heilemann, V. Cornish and M. Sauer, *Nat. Methods*, 2010, **7**, 717–719.
- 18 A. A. Hoskins, L. J. Friedman, S. S. Gallagher, D. J. Crawford, E. G. Anderson, R. Wombacher, N. Ramirez, V. W. Cornish, J. Gelles and M. J. Moore, *Science*, 2011, **331**, 1289–1295.
- 19 P. F. Aramendia, R. M. Negri and E. S. Roman, *J. Phys. Chem.*, 1994, **98**, 3165–3173.
- 20 M. E. Sanborn, B. K. Connolly, K. Gurunathan and M. Levitus, *J. Phys. Chem. B*, 2007, **111**, 11064–11074.
- 21 M. Levitus and S. Ranjit, *Q. Rev. Biophys.*, 2011, **44**, 123–151.
- 22 H. S. Muddana, T. T. Morgan, J. H. Adair and P. J. Butler, *Nano Lett.*, 2009, **9**, 1559–1566.
- 23 M. Y. Berezin and S. Achilefu, *Chem. Rev.*, 2010, **10**, 2641–2684.
- 24 H. A. Kramers, *Physica*, 1941, **7**, 284–304.
- 25 A. Samanta, *et al.*, *Angew. Chem., Int. Ed.*, 2011, **50**, 6089–6092.
- 26 G. Luo, M. Wang, W. H. Konigsberg and X. S. Xie, *Proc. Natl. Acad. Sci. U. S. A.*, 2007, **104**, 12610–12615.
- 27 S. Myong, S. Cui, V. P. Cornish, A. Kirchhofer, M. U. Gack, J. U. Jung, K. P. Hopfner and T. Ha, *Science*, 2009, **323**, 1070–1074.
- 28 L. V. Johnson, M. L. Walsh, B. J. Bockus and L. B. Chen, *J. Cell Biol.*, 1981, **88**, 526–535.
- 29 B. Banerjee, D. Bhattacharya and G. V. Shivashankar, *Biophys. J.*, 2006, **91**, 2297–2303.
- 30 M. J. Hinner and K. Johnsson, *Curr. Opin. Biotechnol.*, 2010, **21**, 766–776.
- 31 B. Fierz, C. Chatterjee, R. K. McGinty, M. Bar-Dagan, D. P. Raleigh and T. W. Muir, *Nat. Chem. Biol.*, 2011, **7**, 113–119.